

Abstract

Abnormal corneal wound healing is a significant medical problem that has been widely addressed in the bioengineering community. It is estimated by the Federal Occupational Health that there are ~ 2.5 million eye injuries in the United States each year, and about 40,000 corneal transplants occur annually, according to the National Eye Institute.

Following surgery or traumatic injury, corneal wound healing can lead to impairment of ocular function via scarring and corneal fibrosis. This fibrosis is caused by the activation of corneal keratocytes from their native quiescent state to an activated my fibroblastic phenotype. This transformation is tied to the release of platelet-derived growth factor (PDGF) upon damage of the basement membrane of the corneal epithelium. Thus, activated by PDGF, the keratocytes begin to secrete extracellular matrix (ECM) proteins and exert elongation forces to help repair the wound. Consequently, however, these behaviors can lead to a disordered tissue microstructure within the corneal stroma, which causes corneal hazing or a reduction in the transparency of the cornea. Although it is well known that the response of keratocytes in corneal wound healing is regulated by both soluble biochemical cues and insoluble biophysical cues (e.g. topography, ECM composition, elasticity) present in the local microenvironment, there are still significant gaps in our knowledge of the factors and mechanism(s) that lead to stromal fibrosis and corneal haze instead of normal wound repair.

Currently, there are no efficient technique that can recreate the orthogonal collagen patterning of the stroma, in the form of a patch in vitro. After laser eye surgery or a keratectomy, there are areas of collagen that have been severed and acellular zones. By creating collagen patches, the biomimicry of wound injury can be modeled for cellular responses due to the release of PDGF. When a section of collagen is severed (i.e. Photorefractive Keratectomy (PRK) or Laster In Situ Keratomileusis (LASIK)).

In this study, we answer the following question: using microfluidic devices can we develop a technique to fabricate

orthogonal collagen patterned patches in vitro?



"The Cornea." *Hybrid Cornea*, www.hybridcornea.org/aboutcornea.htm. **Figure 1.** depicts the layers of the cornea, the relative thickness of each layer are, Epithelial ~50 um, Bowman's ~5 um, Stroma ~500 um, Descemet's membrane ~10 um, and Endothelial ~5 um.

Hypothesis

- By placing an orthogonal poly-dimethyl siloxane (PDMS) microfluidic device on a fabricated collagen line, the underlying collagen layer will be ripped off where it meets the stamp, producing a collagen area of known dimension.
- During normal wound healing *in vivo*, keratocytes are exposed to various stimuli that can have additive, antagonistic, synergistic, or potentiating effects on the keratocyte response.



- We have developed a novel method for creating patches of aligned collagen fibrils of well-defined widths (50-1500 um) that can serve as biomimicry of wound injury.
- We have demonstrated that when keratocytes are cultured on top of these collagen fibrils, there was co-alignment between the keratocytes and the collagen fibrils.
- These substrates can be used to further understand how topography regulates the adhesion and migration of corneal keratocytes during wound healing.

- Use TGF- β_1 to investigate its contractile forces and stress-fibers to further understand corneal wound healing.
- Analyze the interaction between stromal and epithelial wound healing as related to corneal wound healing.
- Investigate fibronectin as it relates to fibroblast adhesion to fibrin substrates and collagen matrices, as it pertains to corneal wound healing.

OI
$$(\theta) = \{2 < \cos^2(\theta) > -1\} * 100\%$$

$$\cos^{2}(\theta) = 1000 * \frac{\int_{-90}^{90} I(\emptyset) \{\cos^{2}(\emptyset - \theta)\} d\emptyset}{\int_{-90}^{90} I(\emptyset) d\emptyset}$$

1. Tuyer-Mai M. Phan, et. al. (1989). Role of Fibronectin and Fibrinogen in Healing of Corneal *Epithelial Scrape Wounds*. Association for Research in Vision and Ophthalmology. 2. William D. Staatz, et.al. (1990). The $\alpha_2\beta_1$. Integrin Cell Surface Collagen Receptor Binds to the α_1 (I)-CB3 Peptide of Collagen. J Biol Chem 3. Kivanany, P.B.; Grose, K.C.; Petroll, W.M. Temporal and spatial analysis of stromal cell and extracellular matrix patterning following lamellar keratectomy. Exp. Eye Res. 2016, 153, 56–64. **Contact & Acknowledgments** For contact: Jacob Adam Awkal, jaa170330@utdalls.edu Acknowledgment: I would like to thank Kevin H. Lam and Tarik Z. Shihabeddin for their encouragement, insight, and enthusiasm during this project. Finally, thank you Dr. Schmidtke for allowing me to pursue a research initiative with the Jonsson School Research Scholars Program in the Schmidtke Lab.